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## Large-scale automated histology in the pursuit of connectomes

David Kleinfeld<sup>1,2</sup>, Arjun Bharioke<sup>3</sup>, Pablo Blinder<sup>1</sup>, Davi D. Bock<sup>3</sup>, Kevin L. Briggman<sup>4</sup>, Dmitri B. Chklovskii<sup>3</sup>, Winfried Denk<sup>3,4</sup>, Moritz Helmstaedter<sup>4</sup>, John P. Kaufhold<sup>5</sup>, Wei-Chung Allen Lee<sup>6</sup>, Hanno S. Meyer<sup>7</sup>, Kristina D. Micheva<sup>8</sup>, Marcel Oberlaender<sup>7</sup>, Steffen Prohaska<sup>7,9</sup>, R. Clay Reid<sup>6</sup>, Stephen J. Smith<sup>8</sup>, Shinya Takemura<sup>3</sup>, Philbert S. Tsai<sup>1</sup> and Bert Sakmann<sup>7,10</sup>

1. Department of Physics, UCSD, La Jolla, CA, USA.
2. Section of Neurobiology, UCSD, La Jolla, CA, USA.
3. HHMI Janelia Farm Research Campus, Ashburn, VA, USA.
4. Max Planck Institute for Medical Research, Heidelberg, Germany.
5. SAIC Intelligent Systems Division, Arlington, VA.
6. Department of Neurobiology, Harvard Medical School, Boston, MA, USA.
7. Department of Digital Neuroanatomy, Max Planck Florida Institute, Jupiter, FL USA.
8. Department of Molecular and Cellular Physiology, Stanford University School of Medicine, Stanford, CA, USA.
9. Department of Visualization and Data Analysis, Zuse Institute Berlin, Germany
10. Max-Planck Institut für Neurobiologie, Martinsried, Germany.

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### Correspondence

David Kleinfeld  
University of California  
9500 Gilman Drive  
La Jolla, CA 92093–0374  
Phone: 858–822–0342  
Email: [dk@physics.ucsd.edu](mailto:dk@physics.ucsd.edu)

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**How does the brain compute? Answering this question necessitates neuronal connectomes, annotated graphs of all synaptic connections within defined brain areas. Further, understanding the energetics of the brain's computations requires vascular graphs. The assembly of a connectome requires sensitive hardware tools to measure neuronal and neurovascular features in all three dimensions, as well as software and machine learning for data analysis and visualization. We present the state-of-the-art on the reconstruction of circuits and vasculature that link brain anatomy and function. Analysis at the scale of tens of nanometers yields connections between identified neurons, while analysis at the micrometer scale yields probabilistic rules of connection between neurons and exact vascular connectivity.**

What are the algorithms that animals use to sample their environment, compute strategies for survival, and control the motion and rhythms of their body? Answers to these questions are essential in neuroscience, the study of how brains work (Bullock, 1993). The nature of these algorithms and the concomitant dynamics that underlie neuronal computations are constrained by the architecture of the particular nervous system. Likewise, the delivery of nutrients to sustain nervous systems and the interactions between neurons and vasculature are constrained by the architecture of the underlying vasculature network. Recent and ongoing technical advances in histology and all facets of imaging suggest that we are entering a renaissance in terms of our ability to decipher these networks. The description of brain networks can be cast as an annotated graph, in which edges correspond to weighted connections between nodes, commonly called a connectome.

An especially simple connectome is the description of blood vessels that supply nutrients to the brain. Each vessel defines an undirected edge, as blood is permitted to flow in either direction. The junction where different vessels meet, which occurs for triplets in the mammalian brain, defines a node. Additional information may be added by annotating individual edges and nodes. For example, each edge in this graph can be labeled with the length and radius of the vessel. A node may be labeled by its association with a control element, such as a pericyte. The connectivity matrix and annotation associated with the vascular connectome, or angiome, is sufficient to calculate flow patterns in cortex.

Neuronal circuits can also be described in terms of a graph. Here, each synaptic connection defines an edge. Pre- and post-synaptic cells form the nodes. In contrast to the case of brain vasculature, a node typically connects to thousands of inputs and outputs, which define the edges. An edge is directed for chemical synapses and undirected for electrical connections. Annotation defines the chemical composition and strength of the synapse along with a multitude of other attributes. Annotation may also be used to record details about the somata. It is important to be mindful that the graphical description of nervous systems has limitations. When the electrical space-constant of a neuron is small compared to the extent of the dendrites, different parts of the neuron may function independently. While this is ordinarily not an issue with cortical

interneurons, it is an issue for cells in which electrical activity in the dendrites is decoupled from that in the soma. This occurs, for example, in starburst amacrine cells in the retina (Euler et al., 2002; Hausselt et al., 2007). In these cases, each neuron may be represented as a superset of nodes and the value of a connectome is retained.

The recent advent of high throughput anatomical techniques offers the realistic possibility of completing neuronal "wiring" diagrams and vascular "plumbing" diagrams of large brains. What are the precedents to compare this work against? With respect to nervous systems, the pioneering serial section electron microscopy study of White *et al.* (White et al., 1986) largely completed the connectome for *Caenorhabditis elegans*, which contains both electrical and chemical synapses. After a hiatus of 25 years, a near-finished wiring diagram based on the original data and new micrographs have been obtained (Varshney et al., 2011). An analysis of the data yields statistical insights into the network along with a hypothesized mapping of circuit motifs for egg laying behavior (Zhang et al., 2008) and pheromone sensing (Macosko et al., 2009). Fractions of underlying neuronal circuitry have been worked out for "simpler" nervous systems and includes circuits for rhythmic neuronal activity, [such as those that drive the heart in \*Hirudo medicinalis\* \(Kristan Jr. et al., 2005\), swimming in \*H. medicinalis\* \(Stent et al., 1978\), swimming in \*Clione limacina\* \(Satterlie, 1985\), and the escape swim response in \*Tritonia diomedea\* \(Getting, 1983; Kleinfeld and Sompolinsky, 1988\), among other stereotypic behaviors \(Delcomyn, 1980; Shepherd and Grillner, 2010\).](#) Yet the dream of a complete connectome in systems more complex than *C. elegans* remains unfulfilled. With respect to brain vascular systems, the statistics of the connections among blood vessels have been addressed in mice (Tsai et al., 2009b), monkeys (Weber et al., 2008), and man (Lauwers et al., 2008) and flow in small pieces of the subsurface vasculature have been examined (Fang et al., 2008). Yet a full pattern of connectivity exists only for the two-dimensional network of pial vessels (Blinder et al., 2010).

In light of past efforts described above, and cognizant of the growing interest in obtaining connectomes across a variety of animals (Bohland et al., 2009; DeFelipe, 2010; Lichtman et al., 2008; Lu et al., 2009; Seung, 2009; Sporns et al., 2005; Swanson and Bota, 2010), we summarize the status of six ongoing projects that utilize high throughput automated histology in the pursuit of brain connectomes.

## **Connectomes Derived from Nanostructural (10 to 100 nm resolution) Data**

We consider a set of projects in which electron microscopy is used to define the connectome that underlies three computations from vision. In each case, the connections between pairs of neurons are mapped to a connectome with a low degree of false positive errors, as erroneous connections are judged to be worse than missing connections. Electron microscopy is required since axons and spine necks can be 50 nm or less in diameter and the structures of interest are densely packed (Sorra and Harris, 2000). Recently developed methods based on scanning electron microscopy offer exceptionally high axial resolution and reliability of throughput, utilizing block face imaging of the tissue (Briggman et al., 2011; Denk and Horstmann, 2004; Knott et al., 2008), while methods based on transmission electron microscopy currently maintain a significant advantage in terms of the speed of imaging (Bock et al., 2011).

As a first example, circuits in the optic lobe medulla of the fly are reconstructed using serial section transmission electron microscopy (ssTEM) and related to motion detection (Chklovskii et al., 2010). A connectome is formed among all cells in the reconstructed volume. Second, the receptive fields of direction-selective ganglion cells in the mammalian retina are measured and, using serial block-face scanning electron microscopy (SBEM) to delineate synaptic connectivity, modeled by the pattern of input from starburst amacrine cells (Briggman et al., 2011). The connectome is restricted to synapses onto neurons that were functionally probed. Lastly, the receptive fields of a set of cortical neurons are assessed physiologically. Then, using serial section electron microscopy (ssTEM), a connectome of their local synaptic interconnections is formed. These data reveal promiscuous connectivity from excitatory pyramidal cells onto inhibitory interneurons (Bock et al., 2011). The latter two studies emphasize that the combination of physiological recordings with subsequent anatomical reconstructions of the recorded neurons is critical to correlate the neuronal function with network structure.

**In search of the mechanism of motion detection: Serial electron microscopy of the fruit fly visual system (Chklovskii et al., 2010).** Visual systems excel at the detection of moving objects. Yet, the circuit that underlies motion detection is not fully

understood. More than fifty years ago, Hassenstein and Reichardt (1956) proposed an elementary motion detector that computes correlations between visual signals offset in time and space (**Fig. 1A**). Their seminal work was followed by theoretical (Adelson and Bergen, 1985; Hildreth and Koch, 1987; Poggio and Reichardt, 1976; Potters and Bialek, 1994) and experimental (Borst and Egelhaaf, 1987; Borst et al., 2005, 2010; Buchner, 1976, 1984; Clark et al., 2011; Egelhaaf and Borst, 1989; Egelhaaf et al., 1989; Egelhaaf and Reichardt, 1987; Eichner et al., 2011; Schuling et al., 1989; Zanker et al., 1999) investigations whose conclusions were largely consistent with the original proposal. However, there has never been a “smoking gun” that identifies particular neurons with the specific computations within the elementary motion detector.

The combination of two lines of experimental evidence suggests that elementary motion detection is performed in the optic lobe medulla in the fly (**Fig. 1B,C**). First, the upstream lamina does not contain directionally selective neurons (Laughlin, 1994; Laughlin and Hardie, 1978; Zheng et al., 2006, 2009). Second, the immediate downstream processing stage, the lobula plate, integrates elementary motion signals over the visual field (Brotz and Borst, 1996; Haag and Borst, 2003; Schnell et al., 2010; Seelig et al., 2010). These suggest that the neuronal mechanism of motion detection may be revealed through a reconstruction of the medulla of the fruit fly. The realization of such a reconstruction is motivated by the small size of the fly, stereotypic brain geometry from fly to fly, and the repeating structure of the medulla column, so that the reconstructed volume needs to include only one repeating column. It is also aided by the availability of genetic tools for physiological manipulations of individual classes of neurons (Pfeiffer et al., 2008), which provides a means to combine structural information with functional studies.

Serial section transmission electron microscopy is used to reconstruct the neural circuits of the optic lobe medulla (Clements et al., 2008). The tissue is cut into a series of 40 nm thick sections through entire depth of the medulla and each section is imaged at  $3 \times 3 \text{ nm}^2$  per pixel across a field of  $90 \times 90 \text{ }\mu\text{m}^2$  as a set of 4K by 4K pixel images that form a mosaic. This resolution reveals individual pre- and post-synaptic sites and permits thin neuronal processes to be traced through the series. The resultant data set across each fly consist of  $2 \times 10^5$  micrographs, or 3 teravoxels. A semi-automated

pipeline with five distinct tasks was developed for high-throughput circuit reconstruction from these data sets (Chklovskii et al., 2010). Registration places the separately acquired images of different sections and different parts from the same section into alignment with each other. Segmentation partitions the stack of images into sets of voxels that define profiles for distinct neurons. Linkages connect adjacent voxels in consecutive sections that belong to the same cell. Proofreading is a manual step to correct errors in the automated reconstruction. Lastly, annotation identifies pre-synaptic and post-synaptic terminals and neuronal classes.

The results of reconstructing ssTEM sections of the medulla column show that it contains several dozen columnar neurons and tens of thousands of synaptic terminals. The connectome was assembled by attributing synapses to specific neurons that were identified by comparing their shape with the light microscopy images of Golgi impregnations (Fischbach and Dittrich, 1989). Finally, most neurons reconstructed with ssTEM could be matched to light microscopy images of transgenic GAL4-UAS lines that expressed green fluorescent protein as an extension of past methods (Pfeiffer et al., 2008). These lines will allow genetic access to neurons of specific classes to determine their repertoire of neurotransmitters and synaptic receptors, manipulate their physiological properties, and monitor their activity. The emerging connectome, along with future physiological investigations, should be sufficient to conclusively resolve the nature of elementary motion detection mechanism in fruit fly, as well as provide insight into the other computations of the visual system.

**The specificity of synaptic connections that underlie direction-selectivity in the mammalian retina (Briggman and Denk, 2006; Briggman et al., 2011; Denk and Horstmann, 2004).** An automated method to acquire volumetric electron microscopy data, SBEM (Denk and Horstmann, 2004), may be used to reconstruct all neuronal structures at resolutions of tens of nanometers. This high resolution is crucial for the reliable tracing of fine neuronal processes in all three dimensions and to ensure that the connections between neurons are inferred with relatively few false positive errors. In this technique, scanning electron microscopy is used to image backscattered electrons from the surface of a plastic embedded tissue block. The top tens of nanometers of a tissue block are first imaged (**Fig. 2A**), the block is then advanced upward and a thin section is

cut from the block-face *in situ* with a custom-made microtome that is mounted within the vacuum chamber of the scanning electron microscope (**Fig. 2B**). This provides a fresh surface for imaging. Repeated imaging and sectioning of the block-face are completely automated.

The specificity of connections from starburst amacrine to direction-selective retinal ganglion cells in the mammalian retina is used to demonstrate the capabilities of SBEM. Both of these cell types are involved in computing the direction of movement. Starburst amacrine cells make inhibitory synapses onto direction-selective retinal ganglion cells. Each dendrite of an amacrine cell is preferentially activated by visual stimuli that move in a particular direction (Euler et al., 2002), while different retinal ganglion cells have different preferred directions. It has been hypothesized, based on the results of physiological studies (Fried et al., 2002; Wei et al., 2010), that On-Off direction-selective retinal ganglion cells gain their direction-selectivity in part by an asymmetric pattern of inputs from directionally-sensitive starburst amacrine cells.

Two experimental steps are required to test this hypothesis. The first is to record the functional response properties of several directionally-sensitive ganglion cells. Two photon laser scanning microscopy (Denk et al., 1990) (TPLSM) was used to image calcium transients in a population of several hundred ganglion cell somata (Briggman and Euler, 2011; Denk and Detwiler, 1999) in response to stimulation with a bar of light that moved in one of eight possible directions. The retina was then fixed and the tissue prepared for SBEM. The second step is to reconstruct the connections in a volume that contained the nearly complete dendritic trees of the recorded cells and their pre-synaptic starburst amacrine cells. The acquired volume,  $60 \times 350 \times 300 \mu\text{m}^3$  at a resolution of  $16.5 \times 16.5 \times 23 \text{ nm}^3$  for a dataset size of 1 teravoxel, contained all of the imaged somata and encompassed the typical diameter of the dendritic tree of retinal ganglion cells. In the example of **Figure 2C**, the dendritic trees for six direction-selective ganglion cells and 24 starburst amacrine cells were manually traced and the synaptic contacts between pairs of cells were tabulated.

The analysis of the reconstructed synaptic contacts revealed that the dendrites of starburst amacrine cells that are oriented along the direction for which the post-synaptic



ganglion cell has a minimal calcium response to motion, *i.e.*, the null direction, are much more likely to form synapses than the dendrites oriented along the direction for the maximum response of the ganglion cell (**Fig. 2C,D**). This result confirms the hypothesis that asymmetric wiring of this circuit is essential for the computation of the direction of motion in the retina. In addition, these studies uncovered evidence that information about the direction of individual starburst amacrine cell dendrites is likely used during development to create the wiring specificity (**Fig. 2E**). While manual methods were used to reconstruct only a small fraction of the neurons contained in the tissue collected for this study, further analysis of this and future volumes of tissue will greatly benefit from the use of high-throughput tracing efforts (Helmstaedter et al., 2011) and automated methods (Jain et al., 2010).

**Anatomy and *in vivo* physiology from a neuronal network in visual cortex (Bock et al., 2011).** In work similar to the above case of circuits in the retina, an understanding of the relationship between function and structure in neuronal circuits of the cerebral cortex is achieved by relating the simultaneous activity of many neurons to the anatomical connections among these cells. To achieve this goal, *in vivo* TPLSM for intracellular calcium measurements (Kerr et al., 2005; Ohki et al., 2005; Stosiek et al., 2003; Svoboda et al., 1997) was combined with large-scale ssTEM to examine the local microcircuit formed by these cells (Bock et al., 2011). The use of TPLSM to record calcium signals, as opposed to microelectrode recordings of cell voltages, permits functional data as well as anatomical landmarks to be obtained. All measurements involved mouse primary visual cortex.

The first step in this process is to characterize the sensory physiology of neurons in visual cortex while the animal watched drifting black and white bars of varying orientations. The animal was then perfused and the brain was removed and processed for ssTEM (Harris et al., 2006). A custom-built camera array was used to acquire data (**Fig. 3A**). For the example of **Figure 3**, a  $450 \times 350 \times 50 \mu\text{m}^3$  volume was sampled at  $4 \times 4 \times 45 \text{ nm}^3$  per voxel; the final set of stitched and aligned data is 10 teravoxels. Brain vasculature served as a fiducial to achieve a cell-level correspondence between *in vivo* imaging and electron microscopy image stacks. In this same example, the proximal dendritic and axonal arbors of 13 physiologically characterized cells were manually

traced. For each synapse along the axonal arbor, the postsynaptic dendrite was traced to either the edge of the ssTEM-imaged volume or to the postsynaptic cell body (**Fig. 3B**). The postsynaptic processes were reliably categorized as either inhibitory or excitatory based on a variety of morphological criteria. This led to a connectome that was annotated with *in vivo* physiology with local network anatomy in cortex (**Fig. 3C**).

The first realization of this process showed that inhibitory cells received convergent anatomical input from diversely tuned neighboring excitatory cells, without apparent regard to orientation selectivity (Bock et al., 2011). This finding is in agreement with intracellular measurements of pair-wise synaptic connectivity (Hofer et al., 2011) and is further consistent with the observation that most inhibitory interneurons show weak or no orientation selectivity (Kerlin et al., 2010; Kuhlman et al., 2011; Liu et al., 2009; Niell and Stryker, 2010; Sohya et al., 2007; Zariwala et al., 2011), although some subtypes may be more selective than others (Ma et al., 2010; Runyan et al., 2010). Finally, when orientation-selective inhibitory neurons are found, their preferred orientation matches the bias shown by neighboring pyramidal cells (Kerlin et al., 2010). Taken together, these anatomical and physiological results suggest a model in which inhibitory interneurons usually pool the activity of nearby pyramidal cells. Continued increases in the number of physiologically characterized cells and the size of the reconstructed volumes should further clarify this issue and are anticipated to uncover additional motifs that link circuit function and anatomical connectivity.

### **Connectomes Derived from Microstructural (0.1 to 1 $\mu$ m resolution) Data**

In studies complementary to the connectomes derived above, the complete inventory of structures in murine cortex is assessed with high-throughput optical tools and protein-specific markers. The molecular signature and structural characteristics of synapses across the depth of cortex, at single-synapse resolution, are revealed by array tomography (Micheva et al., 2010). This serves as essential information to annotate edges in the connectome. Reconstruction of the connections among all blood vessels relative to their surrounding brain cells suggests strategies for synaptic control of blood flow by contractile elements (Blinder et al., 2010). Lastly, the locations of all neuronal somata within a single column, their identification in terms of specific cell types, the

assignment of canonical morphologies, and the estimate of synaptic contacts between different cell types form a connectome based on estimated connectivity, and allow the assessment of putative pathways for self-motion versus touch (Oberlaender et al., 2011a).

**The diversity of cortical synaptic connections as revealed by array tomography (Micheva et al., 2010; Micheva and Smith, 2007).** The connectome involves annotation of synaptic components in addition to a graph that tabulates connections. In the case of neuronal circuitry, as opposed to electrical circuits, the components are extremely diverse and schemes to classify synaptic components are only emerging (Bug et al., 2008). Neuronal cell diversity has been studied intensively since the pioneering morphological investigations of the nineteenth century, and ongoing electrophysiological and molecular studies make it clear that such cellular diversity is enormous, *e.g.*, at least 24 neuronal types in the CA1 region of the hippocampus alone (Klausberger and Somogyi, 2008). Synaptic diversity is an even greater enigma. This occurs because synapses are orders of magnitude more numerous than neurons and because synapses have proved far more difficult than neurons to study at the unitary level. Nonetheless, the limited morphological, gene expression, and proteomic data presently available strongly imply that synapse diversity must be enormous.

Array tomography is a high-resolution proteomic imaging method that provides new opportunities to explore and map synapse molecular diversity (**Fig. 4**). First, array tomography allows individual synapses within brain tissue to be resolved with wide-field fluorescent microscopy at the theoretical maximum for lateral resolution, *i.e.*, ~ 200 nm, and sub-diffraction resolution in the axial direction, *i.e.*, ~ 70 nm, by physically sectioning the samples. Second, array tomography can detect the distribution of dozens of antigens within the same synapse by eluting antibodies and restaining the sample multiple times. The ability to multiplex the binding capability of structural proteins and organelles provides a broader context to decipher molecular architecture than that gleaned through conventional immunofluorescence. Thirdly, array tomography can acquire large volumes, which contain millions of synapses, since both immunological labeling and imaging are not limited by depth within the tissue. The planar images from each section are stitched. While there is no fundamental limit to the final size, current

data sets typically encompass  $1500 \times 500 \times 12 \mu\text{m}^3$  regions with about 20 different molecular markers. As a result of these three features, array tomography data can reveal a previously unseen level of synaptic diversity.

Data acquired by array tomography are represented by “synaptograms” (**Fig. 4C**), which allow the simultaneous display of both the spatial and high proteomic content of each synapse. The columns in a synaptogram represent serial sections through a synapse and the rows represent individual markers. Synapses are classified into subtypes based on the coexpression and spatial relation of a number of relevant markers. For the example of **Figure 4C**, the synaptogram on the left represents a glutamatergic VGlut1 synapse, based on the colocalization of a number of pre- and post-synaptic glutamatergic markers, while the synaptogram on the right contains GABAergic pre- and postsynaptic markers and represents a GABAergic synapse. At least a dozen of different synapse subtypes in mouse cerebral cortex have been identified in this way so far, using neurotransmitter, vesicular transporter, calcium binding protein and receptor markers. Manually classified synapse samples are used to train machine-learning algorithms for automatic classification and quantification of all synapses within the sample (**Fig. 4D**). Lastly, synapse subtypes can be related to their parent neurons through the use of transgenic animals that express fluorescent proteins in specific neuronal subsets (Feng et al., 2000) or in individual neurons (Li et al., 2010).

The details of synaptic diversity as observed with array tomography represent only a snapshot of the state of brain synapses at a fixed moment of time. However, it may be possible to address temporal changes in synaptic proteomics that relate to activity levels, plasticity, circadian rhythms, and development by a combination of live imaging followed by array tomographic analysis of the same tissue. In this way, potentiated synapses at dendritic spines (Murakoshi et al., 2011) or newly formed spines during learning (Xu et al., 2009; Yang et al., 2009) could be analyzed to find the molecular signatures defining a potentiated or newly formed synapse. In the simplest form, one can analyze synapses that emanate from neurons that were previously filled with dye. In this way, the scope of array tomography can offer a dynamic view of synapse composition and diversity that is integrated into a neuronal circuit schematic.

**Dynamics and control of cortical blood flow in relation to the angiome (Blinder et al., 2010; Tsai et al., 2003; Tsai et al., 2009b).** The cerebral vascular system services the constant demand for energy during neuronal activity in the brain. The determination of the geometry of this network is mandatory to understand how neurovascular control elements modulate the distribution of blood flow in the brain and, by extension, how to interpret the signals from functional magnetic resonance imaging (fMRI) techniques that infer the activation of neurons based on changes in blood flow and oxygenation. It has been suggested that the vasculature in mammalian cortex is organized as modules around neuronal units and thus has a columnar organization (Duong et al., 2001; Duvernoy et al., 1981; Lauwers et al., 2008; Zhao et al., 2005). However, fMRI-based studies do not achieve sufficient spatial resolution to analyze the underlying microvascular structure. For example, Bolan and coworkers (Bolan et al., 2006) attained a resolution of  $24 \times 24 \times 78 \mu\text{m}^3/\text{voxel}$  across the brain, which was sufficient to resolve major arteries and veins but insufficient to resolve microvessels (Tsai et al., 2009b). In addition, high resolution anatomical studies of the human (Cassot et al., 2006; Lauwers et al., 2008) and primate brain vasculature (Weber et al., 2008) were not colocalized with cortical columns. To achieve the necessary combination of resolution and spatial extent, as well as colocalization of vessels and neurons, all optical histology (Tsai et al., 2003) was used to simultaneously acquire datasets of the vasculature and the cytoarchitecture of the murine primary somatosensory cortex (**Fig. 5A**).

All optical histology combines TPLSM and plasma-mediated ablation (Oraevsky et al., 1996; Tsai et al., 2009a) to sequentially image and remove portions of the tissue (**Fig. 5B**). This process of imaging and ablation is repeated iteratively to acquire volumes of several cubic millimeters, with separate channels for different fluorescent indicators, e.g., a fluorescein-conjugated gel that fills the lumen of all vasculature, DAPI that stains all nuclei, and rhodamine-conjugated to the pan neuronal marker  $\alpha\text{NeuN}$  to identify neuronal nuclei. This method was used to reconstruct the entire vasculature around several cortical columns in primary vibrissa cortex of mouse, *i.e.*, “barrel” cortex, (Fox, 2008; Lefort et al., 2009; Woolsey and Van Der Loos, 1970), in which the input from a single facial macrovibrissa is conveyed by a set of highly organized thalamic afferents into a respective cortical column (Meyer et al., 2010b; Van Der Loos, 1976; Wimmer et al., 2010). Images were obtained at  $1 \times 1 \times 1 \mu\text{m}^3$  sampling to yield data sets

of 1 gigavoxel per channel for a cubic millimeter. The raw gray-scale data for each channel is processed to obtain a vectorized representation. The vasculature is transformed into an angiome with the edges, *i.e.*, vessel segments, annotated by their length and radius. All cell nuclei are represented by their centroid coordinates and are classified as neurons or non-neurons (Tsai et al., 2009b). One critical aspect of this process is the stitching of data blocks in all three dimension (**Fig. 5B**). A second is the correction of gaps in the vascular data, for which a threshold-relaxation algorithm connects nearby ends when the gel in the lumen contains a discontinuity (Kaufhold et al., 2008) (**Fig. 5C**). Finally, the data on neuronal positions is used to determine the location of columnar boundaries (**Fig. 5D**).

The pial vasculature of cortex forms a fully connected two dimensional graph that robustly transports blood across the cortical mantle (Schaffer et al., 2006) (**Fig. 5E**). Here, as with all aspects of the cortical vasculature, the coordination at each vertex is three. Blood is actively redistributed from regions with low need to those with high need (Blinder et al., 2010; Devor et al., 2007). The neurons are fed by a subsurface network of tortuous microvessels that form a fully connected graph. The surface vasculature network connects to the subsurface microvasculature through a series of penetrating vessels (**Fig. 5E**). There are fewer penetrating arteries than 'barrels', providing evidence against the notion of a microvascular unit that overlays a column. The issue of structural domains in the microvasculature was addressed by an exhaustive search for a statistically meaningful partition of this network (Frey and Dueck, 2007). By definition, structural modules will have higher inter-connectivity between vertices within a module than between vertices of different modules. Overall, no significant topological clusters were identified; neither in the entire microvasculature nor in layer IV separately. These findings suggest that neuronal units are embedded in a continuum of microvessels. Thus, local regulation of perfusion, and not the vasculature structure itself, governs the flow patterns observed by fMRI.

**Cell type-specific reconstruction of the rodent brain at cellular resolution (Lang et al., 2011; Meyer et al., 2010a; Oberlaender et al., 2011b; Oberlaender et al., 2009b).** Reverse engineering of the cortical column provides a means to link an anatomically realistic network model, in which the structure of neurons and both the short- and long-

range synaptic wiring among different cell types conform with anatomical reconstructions, to the flow of electrical signals in the column (Helmstaedter et al., 2007; Lang et al., 2011). This reconstruction program involves four essential steps (Oberlaender et al., 2011b): (i) reconstruction of the spatial locations of neuronal somata in large brain structures, independent of the type of cell; (ii) assignment of a type to each neuronal somata; (iii) reconstruction of the dendritic and axonal projection patterns for each type of neuron; and (iv) estimation of the synaptic connections based on the probability of overlap between dendrites and axons. The connections between cells are thus known only probabilistically. The focus is on the cortical columns in vibrissa cortex of rodent, as was the case for the vascular connectome (**Fig. 5E**).

The first step, reconstruction of the location of all neuronal somata, proceeds by labeling sections with  $\alpha$ NeuN to specifically visualize all neuronal nuclei. Manually detected somata in high-resolution confocal image stacks led to a measurement of the density of neurons within entire columns in rat (**Fig. 6**); the resulting neuron numbers per layer in the average column were 60, 2000, 3700, 4400, 1700, 2200, 3800, and 1100 for layers 1, 2, 3, 4, 5A, 5B, 6A, and 6B respectively, for a total of 19,000 neurons per cortical column (Meyer et al., 2010a).

An automated image processing pipeline facilitated a combined analysis of the first two steps, reconstruction of the location of neuronal somata and the assignment of a cell type to each neuron, within an entire rodent brain (Oberlaender et al., 2009a). In the example of **Figure 7** for mouse cortex, sections were labeled with antibodies against GAD67, to specifically visualize GABAergic interneurons, in addition to  $\alpha$ -NeuN (Meyer et al., 2011). Reconstruction of the distribution of excitatory and inhibitory neurons is achievable from 210 serial sections that were 50  $\mu$ m thick. High-speed confocal microscopy at 0.36 x 0.36 x 0.6  $\mu$ m<sup>3</sup> resolution was used to form a mosaic of images across an entire section (**Fig. 7B**), resulting in files of ~ 60 gigavoxels per section per channel or ~ 25 teravoxels per mouse brain. The end result is the set of position landmarks of all excitatory and inhibitory neuron somata (**Fig. 7C,D**). Semi-automated post-processing of the image stacks can be used to compensate for tissue preparation artifacts, such as tilt or local distortions of individual brain sections (**Fig. 7E**) and the alignment of consecutive serial sections with cellular precision (**Fig. 7F**). The resultant

high-resolution image stack comprises the entire mouse brain and allows its reconstruction at cellular resolution (**Fig. 7G**).

For the third step, the spatial distribution of cell types within a brain region may be determined by post-hoc anatomical reconstructions of dendrite and axon morphologies (Oberlaender et al., 2011a; Oberlaender et al., 2009a; Oberlaender et al., 2007; Oberlaender et al., 2011b) and by co-localization of neuron somata in transgenic mouse lines where specific cell types express a fluorescent protein (Groh et al., 2010). The final, fourth step is to assemble an average circuit model that combines the locations of all neurons in the reconstructed large brain areas with tracings of cell type-specific dendritic and axonal projections. The synaptic connectivity between neurons within the column and with intercolumnar projections are then estimated from the density of the overlap between axons and dendrites to form an anatomically realistic circuit (Oberlaender et al., 2011b).

In time, the serial section and block face techniques described earlier (**Figs. 2 and 3**) may advance to the stage where entire cortical columns may be exactly reconstructed. This should reveal the nature and magnitude of possible deviations from the statistical view of connectivity. One possibility, implied by findings from studies on neuronal connectivity measured in brain slices (Ko et al., 2011; Otsuka and Kawaguchi, 2009; Perin et al., 2011; Song et al., 2005; Thomson et al., 2002), is that cortical neurons have biases in their connectivity and that some connections may be particularly strong. However, findings with slice preparations can be biased as a consequence of lesioned connections. For now, the circuits derived by this statistical approach provide the state-of-the-art basis for large-scale numerical simulations of sensory-evoked signal flow in a cortical column ([www.neurodune.org](http://www.neurodune.org)) (Lang et al., 2011).

## **Epilog: Computation and Connectomes**

The computational capabilities of a neuronal circuit, and the patterns of electrical activity generated by that circuit, are constrained by the connectome. At the very minimum, the wiring diagram specified by the connectome can be used to distinguish among



algorithms that support a particular computation (Seung, 2009). Lessons from past theoretical work and the analysis of simpler nervous systems provide some guidance on this issue. Tree- or bus-like architectures are suggestive of Perceptrons (Minsky and Papert, 1969), in which the output of a single cell depends on the summation of weighted inputs. This is a canonical model for receptive fields based on summation across a set of receptors (Zipser and Andersen, 1988), of which the Reichardt motion detector is a particular example (Hassenstein and Reichardt, 1956). Sparse feed-forward networks can function as synfire chains (Abeles, 1982), in which sparse spike activity hops along clusters of connected neurons. This is a potential model for temporal sequence generation in bird song (Long et al., 2010). In contrast, feedback loops formed by recurrent neuronal connections can support multiple patterns of persistent activity and are conjectured to be used as memories (Hopfield, 1982; Seung, 2009) and as control structures (Seung, 1996). In the simplest case, triplets of neurons with unidirectional wiring can function as a three-phase clock (Kling and Szekély, 1968); this arrangement forms the aforementioned pattern generator for swimming in leech (Kristan Jr. et al., 2005; Stent et al., 1978). Studies on larger recurrent networks, such as the stomatogastric rhythm generator in crustaceans, provide qualitative support for the notion that a network can support multiple patterns of persistent activity (Marder and Bucher, 2007; Miller and Selverston, 1982). Contrariwise, different connectomes that realize the same recurrent network topology can support identical mean patterns of activity (Amit, 1989; Sompolinsky, 1988).

Considerable effort was spent toward mapping specific neuronal computations, primarily in vision, onto network architectures (**Figs. 1 to 3**). All of these involve large nervous systems that enjoy the advantage of genetic manipulation. Yet one must consider the potential value in revisiting the analysis of a simple system, such as leech. Further, while much current emphasis in high throughput anatomy is placed on connectomes, it would be foolish to dismiss anatomical tracing efforts that take a purely mesoscopic approach (Bohland et al., 2009; Swanson and Bota, 2010). In support of the latter possibility, recent work considered the computational capabilities of a model of the primate visual system based only feed-forward connections between brain regions (Serre et al., 2007). This model could be used to successfully detect a range of salient features in the visual field, such as a person walking into the street. All told, given the

results reported here and the potential value of extensive data sets on all scales, cautious optimism is called for in the realization of connectomes, and associated angiomes, across different species and brain areas.

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## Figure captions

**Figure 1.** Motion detection circuit in fruit fly. **(A)** Hassenstein-Reichardt elementary motion detection compares correlations in light intensity signals offset in space and time. **(B)** Fruit fly. **(C)** A light microscopic section through fruit fly optic lobe showing the first three stages of visual processing: lamina, medulla, and lobula plate. **(D)** Electron microscopy reconstruction of a medulla column, different colors correspond to different neurons. Panel C is adapted from (Takemura et al., 2008).

**Figure 2.** A schematic view of serial block-face scanning electron microscopy technology. **(A)** The electron beam first raster scans the surface of a tissue sample that is embedded in a plastic block. **(B)** After the acquisition of an image acquisition, a diamond knife cuts a thin section from the surface of the block. **(C)** A cutaway of the volume of mouse retina acquired for the study of the direction-selectivity circuit in retina. The image shows a reconstructed starburst amacrine cell in black and the locations of its synapses (see inset) onto direction-selective retinal ganglion cells. The synapse locations are color-coded by the functionally recorded preferred directions of the direction-selective retinal ganglion cells. The scale bar is shorter near the top as a consequence of perspective. **(D)** Starburst amacrine cell somata (large blue and cyan dots) and the direction of their dendrites (blue and cyan vectors) that form synapses (small blue and cyan dots) onto a direction selective ganglion cell (gray). **(insert)** A polar histogram of the vector directions (black) indicate an asymmetric distribution opposite to the functionally recorded preferred direction of the ganglion cell (purple tuning curve). **(E)** Schematic wiring diagrams of starburst amacrine cell input to direction selective ganglion cells for 3 different locations of the starburst cell soma. The starburst cell dendrite directions are biased toward the null direction (ND). Panels A and B are courtesy of Julia Kuhl. Panels C, D and E adapted from (Briggman et al., 2011).

**Figure 3.** The process of realizing a connectome from the network anatomy for mouse visual cortex. **(A)** Custom camera array for transmission electron microscopy. Labeled components: 1, motorized positioner knobs; 2, lead shielding; 3, vacuum chamber extension; 4, scintillator; 5, leaded glass; 6, 2 by 2 array of f/2.0 optical lenses coupled to 50 MHz readout of 11 megapixel CCD cameras; 7, camera trigger breakout box; 8, cables to four acquisition computers. **(B)** Acquisition and reconstruction overview. Top row, left to right: four cameras with overlapping

fields of view of the scintillator; raw camera images; normalized, stitched, and cropped camera images into a single 'tile'. Bottom row, left to right: mosaic of tiles resulting from sample motion; stitched mosaic, with red square delineating zoom area in the next image; zoom of a single tile showing area tracing. Not shown: imaging of multiple sections, alignment of serial section mosaics, tracing through multiple sections, and validation of tracing. **(C)** Three-dimensional tracing of the 14 physiologically characterized cells and their postsynaptic targets; only those targets receiving convergent synaptic input from two or more physiologically characterized cells are shown. Physiologically characterized orientation preference for the cell given in the key, bottom right. **(D)** Connectivity graph of the anatomical objects shown in panel C. Magenta targets are excitatory; cyan targets are inhibitory. Circles are postsynaptic dendrites that could be traced back to the cell body; squares are dendrites that left the imaged volume before the cell body was reached. Panels C and D adapted from (Bock et al., 2011).

**Figure 4.** Array tomography allows the resolution, classification and quantification of individual synapses. **(A)** The array tomography proteomic imaging cycle involves multiple rounds of immunostaining, imaging and antibody elution and allows collection of immunofluorescence data of multiple antibody channels; 24 demonstrated to date. **(B)** Volume rendering of layer 5 of the somatosensory cortex of a Thy-1 YFP-H mouse (Feng et al., 2000), immunolabeled for the general synaptic marker synapsin. Individual synapsin puncta have been segmented digitally and rendered in random color to emphasize that each synapsin punctum is fully resolvable in all three dimensions. Scale bar, 10  $\mu\text{m}$ . **(C)** High dimensional proteomic data are viewed as "synaptograms" with columns representing individual serial sections through a synapse and rows representing each marker. The two synaptograms show examples of a glutamatergic synapse with glutamatergic markers boxed in red and a GABAergic synapse with the respective markers boxed in blue. Each square represents an area of  $1 \times 1 \mu\text{m}^2$ . **(D)** The density of 6 synapse subtypes in the somatosensory cortex of a C57BL/6J mouse plotted as a function of depth through the cortical layers, white matter (WM) and part of the striatum (STR).

**Figure 5.** Cortical angiome and its relation with neuronal columns revealed with all optical histology. **(A)** Gelatin-based fluorescent vascular cast of the entire vasculature of the mouse brain. **(B)** Schematics of all optical histology block-face imaging. A sample that contains one or more fluorescently labeled structures is imaged by TPLSM to collect optical sections through the ablated surface. Sections are collected until scattering of the incident light reduces the signal-to-

noise ratio below a useful value. The top of the now-imaged region of the tissue is cut away with amplified ultrashort laser pulses to expose a new surface for imaging. The sample is again imaged down to a maximal depth, the new optical sections are added to the previously stored stack, and the process of ablation and imaging is repeated. This process generates thousands of overlapping blocks that are stitched together to generate a contiguous volumes. The position of each block on the global coordinate system is determined by the least-square solution of a minimization problem defined by all cross-correlations between overlapping blocks. **(C)** The raw images are vectorized by fitting the data to tubes. However, sections of low signal-to-noise along the vasculature can result in 'gaps', several to tens of micrometers in length, in the reconstructed microvasculature. These are corrected with an automated technique. Left: a region of low signal-to-noise (arrowhead) and the resulting 'gap' (arrow) seen in the max-projections of the gray scale data and its volumetric representation (red isosurface) as well as in the vectorization (red tubes). Center: automated local threshold relaxation finds a bridging mask (cyan, arrow). Right: a corrected vectorization is computed through the gap (red tube, arrow). **(D)** Localization of cortical columns ('barrels') in using data on all fluorescently labels neurons (no shown). Top; axially oriented maximal projections across 50  $\mu\text{m}$  of of the microvasculature on layer IV. Middle: Cell somata using fluorescent channels for a fluorophore linked to the panneuronal antibody  $\alpha\text{NeuN}$  in the same data set as the vasculature; columnar boundaries are distinguished in somata channel but not in the vasculature. Bottom: columns outlines from the cell densities in the middle panel and labeled per convention. **(E)** Vectorized reconstruction across a 1.5  $\text{mm}^3$  volume of somatosensory cortex; same data set as in panel D.

**Figure 6.** Manual detection of neuronal somata in cortical columns from vibrissa cortex of rat. **(A)** Overlay of a maximum-intensity  $\alpha\text{-NeuN}$  fluorescence image with markers that were manually placed at the midpoints of  $\alpha\text{-NeuN}$ -positive somata. **(B)** All NeuN-positive somata in the C2, D2 and D3 columns, defined by extrapolation of the barrel outline in L4 along the vertical axis. **(C)** One dimensional profiles of  $\alpha\text{-NeuN}$  density along the respective vertical column axis for the C2, D2, D3, and the mean column. Adapted from (Meyer et al., 2010a).

**Figure 7.** Automated methods to reconstruct an entire mouse brain at cellular resolution. **(A)** The brain is cut along the coronal into  $\sim 210$  consecutive sections. **(B)** Sections are labeled within  $\alpha\text{-NeuN}$  (red) and  $\alpha\text{-GAD67}$  (green) and imaged as a mosaic with using high-speed confocal microscopy. **(C)** Enlargement of one into box in panel B. **(D)** Enlargement of one box in

panel C. Excitatory (yellow) and inhibitory (pink) somata are detected and labeled using an automated image processing pipeline. **(E)** Tilt and/or distortions of individual brain sections are corrected by semi-automated post-processing. **(F)** The quality of each image stack after post-processing is sufficient to align consecutive sections with cellular precision. **(G)** The resultant image stack comprises the entire mouse brain and allows segmentation of anatomical structures, *e.g.*, blood vessels or pia (brown) and quantification of soma densities (green).

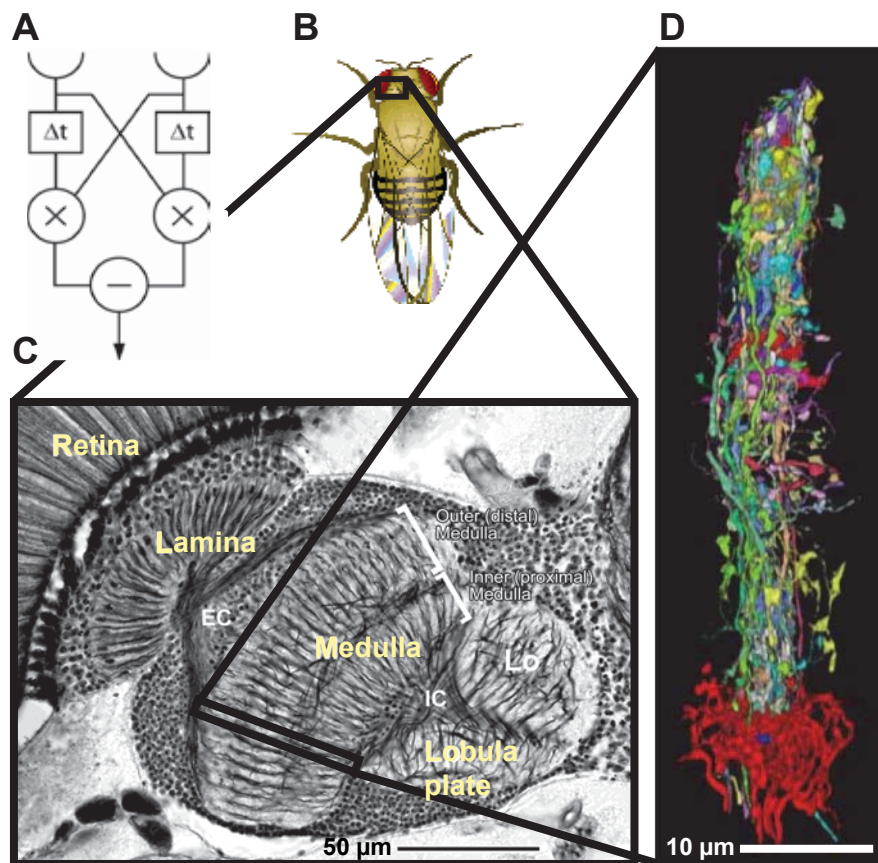


Figure 1. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)



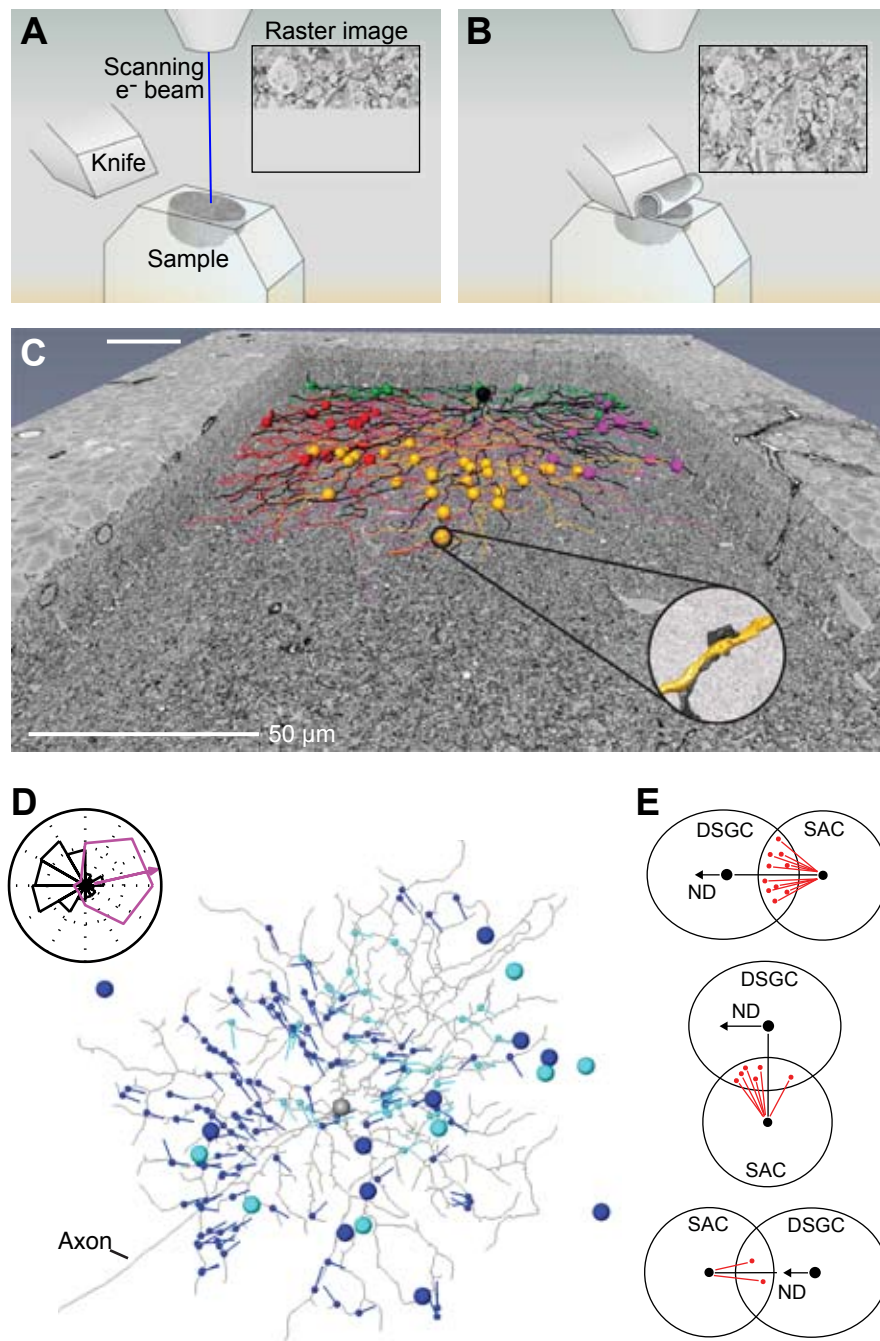


Figure 2. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)

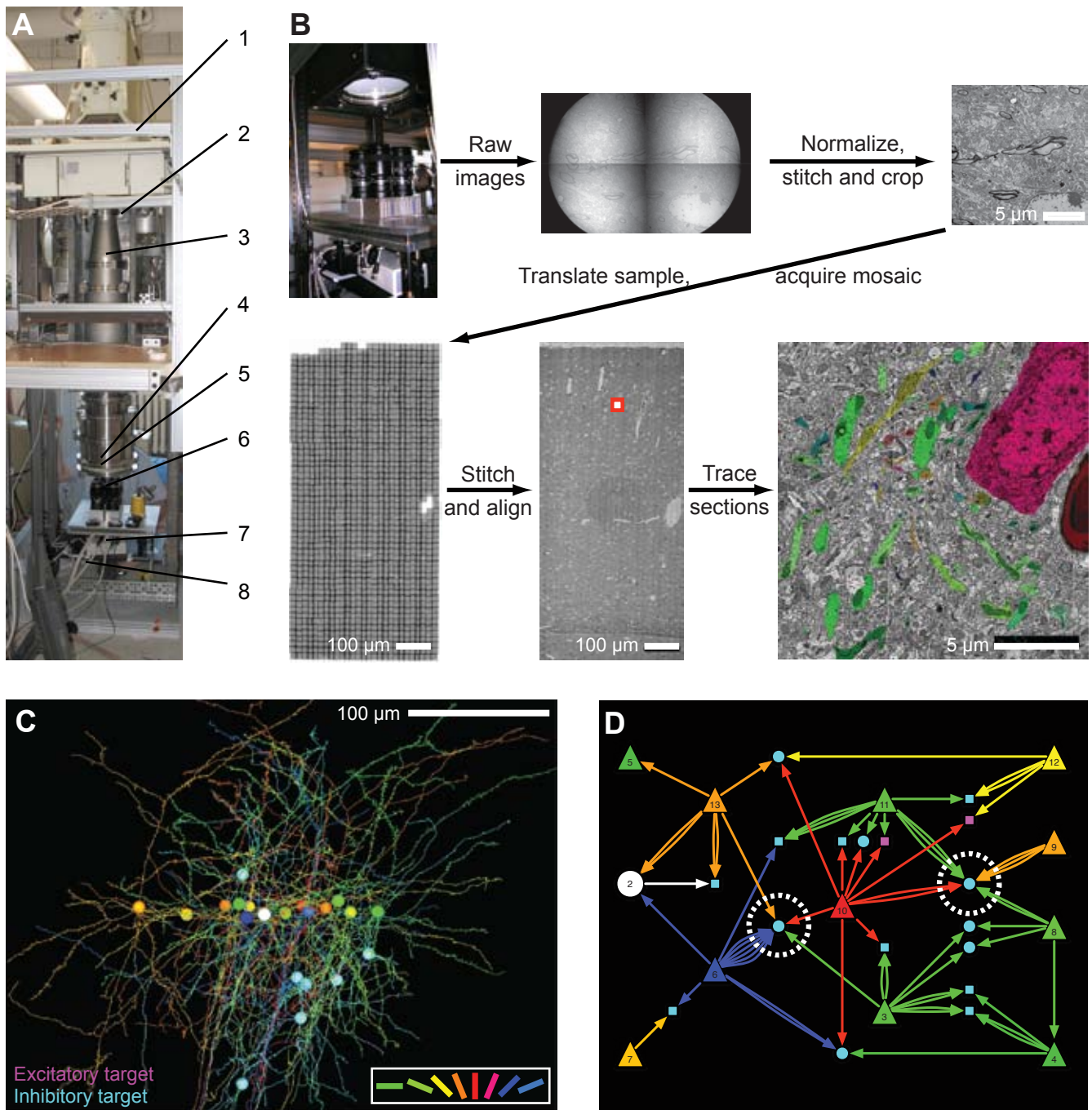


Figure 3. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)

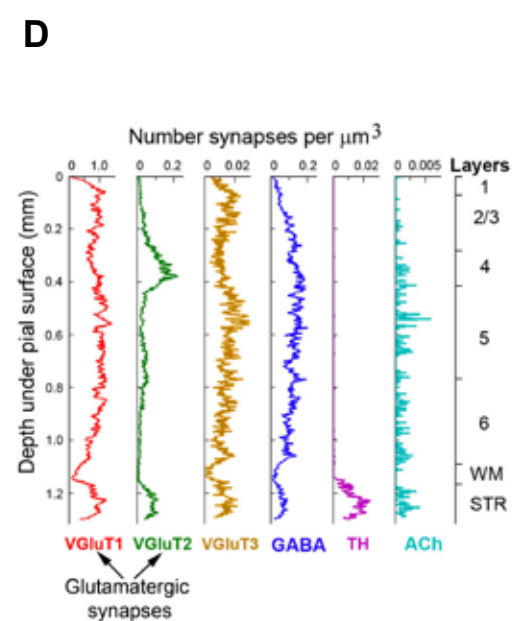
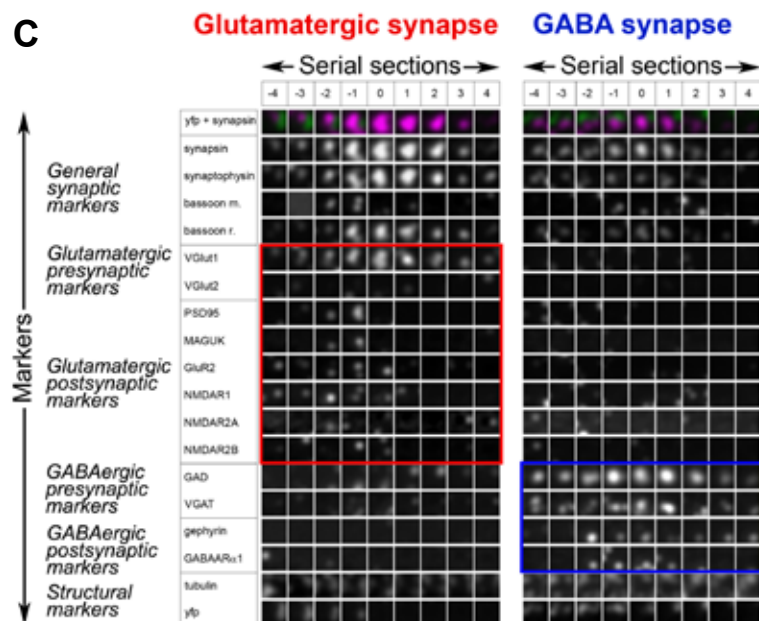
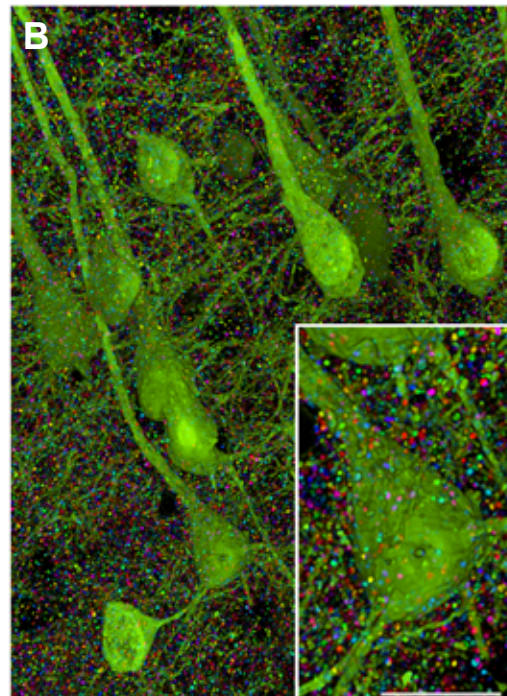
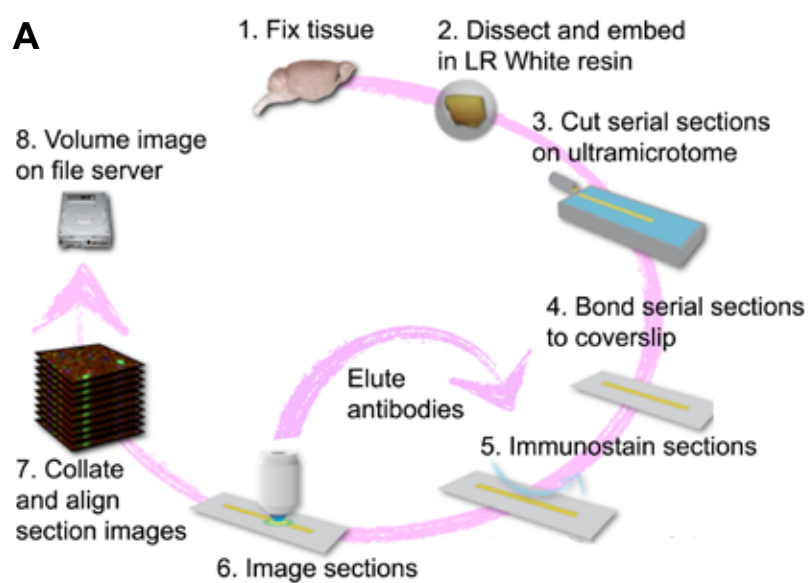


Figure 4. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)



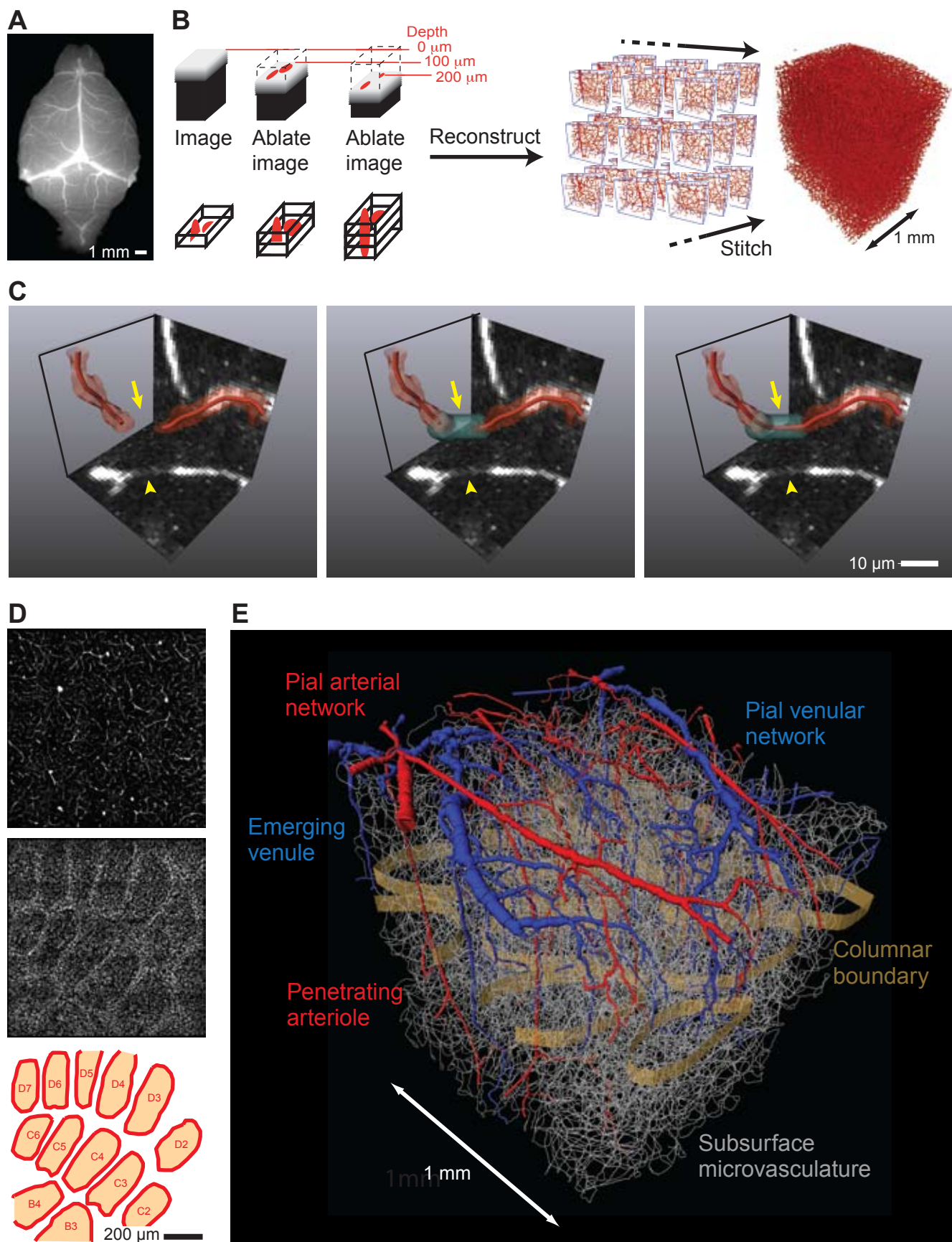


Figure 5. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)

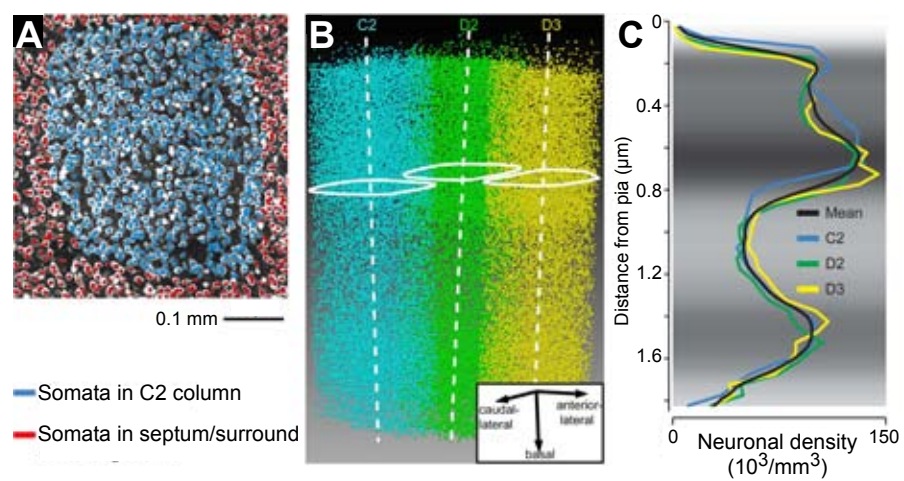


Figure 6. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)



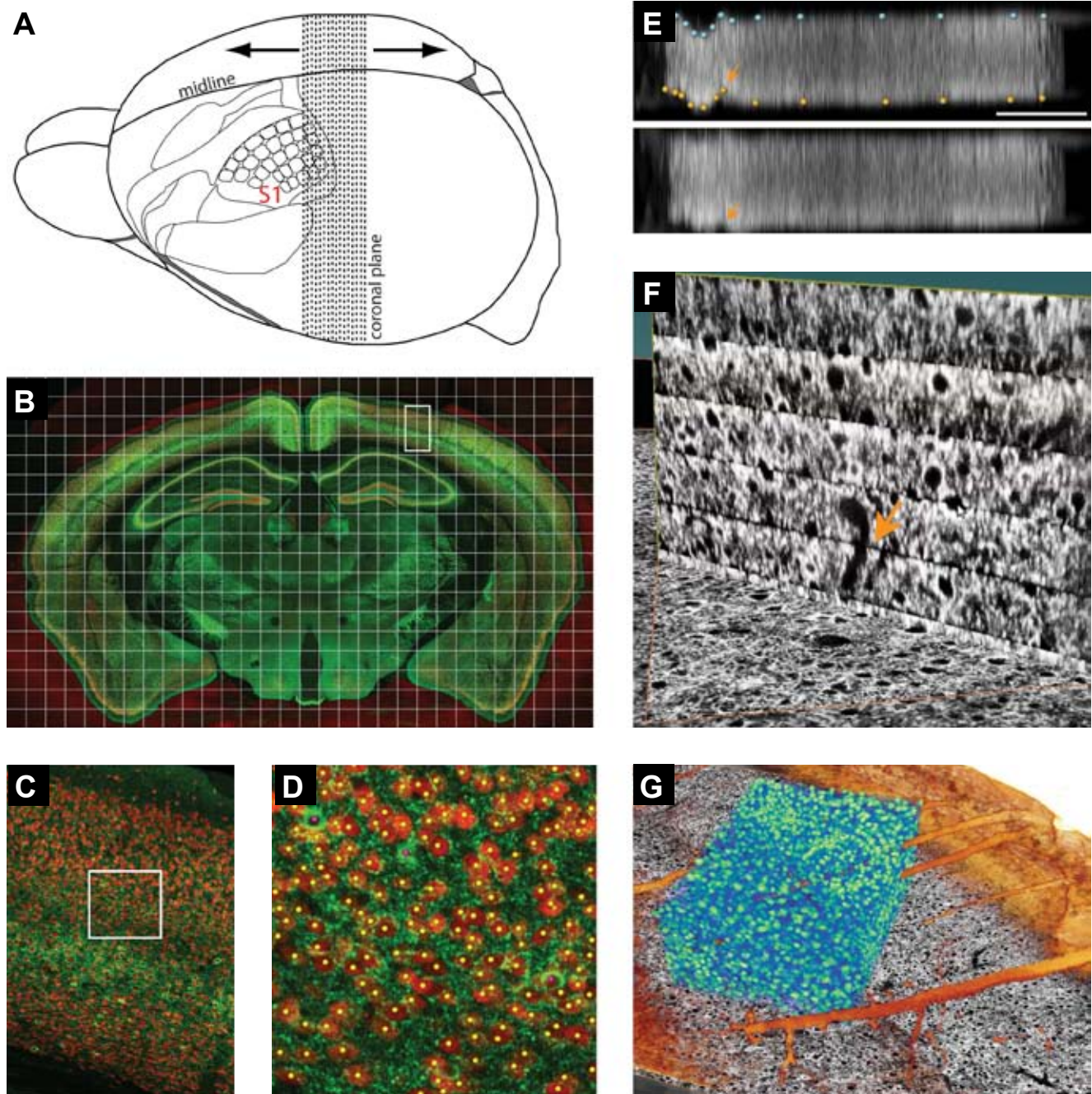


Figure 7. Large-scale automated histology in the pursuit of connectomes (Journal of Neuroscience 2011)